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SYNTHESIS AND FUNCTIONAL EVALUATION OF  
PEPTIDE MODIFIED POLY (LACTIC-CO-GLYCOLIC ACID) NANOPARTICLES  
TO INHIBIT  
PORPHYROMONAS GINGIVALIS BIOFILM FORMATION

By

Paridhi Kalia  
B.D.S., Bhavnagar University, 2012

A Thesis  
Submitted to the Faculty of the  
School of Dentistry of the University of Louisville  
in Partial Fulfillment of the Requirements  
for the Degree of

Master of Science  
in Oral Biology

Department of Oral Immunology and Infectious Disease  
School of Dentistry  
University of Louisville  
Louisville, KY

December 2015

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DEDICATION

To my brother Akshay Kalia

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## ABSTRACT

### SYNTHESIS AND FUNCTIONAL EVALUATION OF PEPTIDE-MODIFIED POLY(LACTIC-CO-GLYCOLIC ACID) NANOPARTICLES TO INHIBIT *PORPHYROMONAS GINGIVALIS* BIOFILM

Paridhi Kalia

Dec 01, 2015

Periodontal disease is an oral inflammatory disorder that afflicts roughly 46% of the adults in the U.S. Currently, treatment of periodontal disease involves the removal of plaque from the gingival pocket (with possible antibiotic treatment) and if necessary, gingival surgery. To our knowledge, no therapeutic approach exists that promotes host-biofilm homeostasis by limiting pathogen recolonization of the oral cavity after prophylaxis or treatment. The interaction of the pathogen *Porphyromonas gingivalis* with commensal streptococci is critical for initiation of periodontitis and represents a target for limiting *P. gingivalis* colonization of the oral cavity. Previous studies showed that a synthetic peptide (BAR) derived from antigen I/II protein of *Streptococcus gordonii* potently inhibited *P. gingivalis* adherence to streptococci. However, BAR was less effective in preventing *P. gingivalis* adherence in a more complex three species biofilm model, suggesting that the potency of BAR against complex biofilms may be reduced. This study focuses on designing surface-modified poly(lactic-co-glycolic acid; PLGA) nanoparticles (NPs) that are functionalized with BAR to increase its inhibitory potency by multivalent binding with *P. gingivalis*. Biotinylated BAR was conjugated to the surface of avidin-palmitylated PLGA NPs. We generated NPs with particle size of 100

$\pm 28$ nm and Zeta Potential of -12mV. The surface modification of avidin-NPs with BAR was examined using two approaches. Comparing the binding of biotin-PEG FITC with avidin-NPs and avidin-NPs that were reacted with biotinylated BAR showed that BAR binding efficiency was approximately 98%. In addition, reacting avidin-NPs with fluorescently labeled BAR showed that a concentration of 37.1 nmol BAR/mg NPs resulted in maximal BAR binding. We also showed that BAR-NPs bound to *P. gingivalis* in a dose-dependent manner and significantly ( $P < 0.01$ ) inhibited *P. gingivalis/S. gordonii* biofilm formation (50% inhibitory concentration =  $0.29 \mu\text{M}$ ) making it 4.5 times more potent than soluble BAR. Together this platform represents a potential therapeutic approach to effectively target an initial interaction involved in *P. gingivalis* colonization of the oral cavity.

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## CHAPTER 1

### INTRODUCTION

According to the World Oral Report 2003, periodontal disease is among the most common microbial disease affecting the adult population worldwide and is one of the major oral health care problems globally. Periodontal disease is prevalent and occurs in 46 % of adults in the U.S.<sup>16,24,15</sup> Severe disease (subgingival pocket depths > 6mm) occurs in 9% of U.S. adults<sup>1</sup> and 11.2% of adults worldwide<sup>16,24</sup>. Domestically, this correlates to annual expenditures for the treatment and prevention of periodontal disease in excess of 14 billion dollars<sup>16,15</sup>.

Periodontal disease is an oral inflammatory disorder that is initiated by microbial biofilms that form in the subgingival pocket leading to severe chronic inflammation characterized by alveolar bone resorption and subsequent tooth loss<sup>21</sup>. The milder form of disease starts with gingival inflammation, termed as gingivitis. Gingivitis, if left untreated can lead to a more severe form of periodontal disease characterized by clinical attachment loss, termed as periodontitis<sup>21</sup>.

#### **Role of Periodontal Pathogens**

The resident organisms of dental plaque play a significant role in the onset and advancement of periodontal disease.<sup>8,22</sup> Over 700 different species of bacteria colonize and interact with each other to form dental plaque<sup>14</sup>. In a state of health, the oral cavity is comprised of benign commensals, majorly *Actinomyces* and streptococci<sup>22</sup>. However

shifts in population, mainly gram-negative anaerobes may orchestrate periodontal disease. Even if these organisms are present in low abundance, they have they have the ability to remodel their local environment from a naturally benign microbiota to a dysbiotic environment<sup>9,10,22</sup>. Among such organisms, *Porphyromonas gingivalis* have gained much attention<sup>9,10,18</sup>.

*P. gingivalis* colonizes in the subgingival plaque, but before transitioning in its primary niche, it first establishes itself in a relatively aerobic environment, where it interacts with commensal streptococci *gordonii*<sup>12,28</sup>. The interaction is mediated by two receptor-ligand pairs namely the the long and short fimbriae of *P. gingivalis*<sup>4,12,28</sup>. The long fimbrial subunit protein (FimA) interacts with cell surface glyceraldehyde-3-phosphate dehydrogenase of *S. gordonii*<sup>8,9,10,12</sup> whereas the minor fimbrial protein in *P. gingivalis*, interacts with streptococcal SspB<sup>5,10</sup>. SspB belongs to the cell surface protein in the antigen I/II protein that are present on the cell surface of nearly all the species of streptococci.<sup>8,9,10,12</sup> . Prior studies suggested that purified *P. gingivalis* showed binding specificity with streptococci *gordonii* primarily because the Mfa1 of *P. gingivalis* did not interact with antigen I/II of *S. mutans*<sup>10</sup>. Furthermore, studies by Demuth et al.<sup>12</sup> and Cook et al.<sup>6</sup> showed that the interaction of *P. gingivalis* and *S. gordonii* mediated by Mfa1-SspB represented an essential initial event that facilitates *P. gingivalis* colonization in the oral cavity.<sup>9,10,18,28,36</sup>

### **Dental Plaque Formation and Disease Pathogenesis**

Dental plaque is a specific and highly variable structural entity consisting of microorganisms and their products embedded in a highly organized intercellular

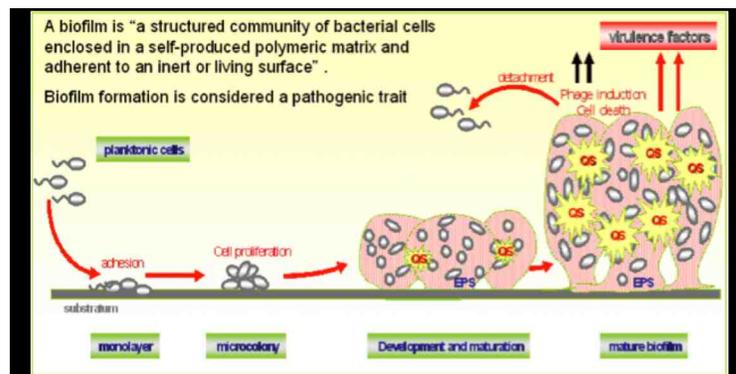
matrix<sup>34,38</sup>. It represents a community of microorganisms involved in a wide range of physical, metabolic and molecular interactions organized in an extracellular matrix<sup>32,33,34</sup>. This environment provides advantages to the organisms such as a broader habitat range for growth and enhanced resistance to antimicrobial agents and host defenses<sup>32,33,34</sup>. Understanding the formation and progression of dental plaque and hence, periodontal disease etiology will aid in developing novel therapies to prevent and treat periodontal diseases<sup>32</sup>.

The process of dental plaque formation is complex, and involves several distinct phases, beginning with bacterial attachment to the tooth surface via the salivary pellicle that forms immediately following tooth eruption or tooth cleaning<sup>13</sup>. Following initial

attachment, adherent bacteria begin to proliferate and form microcolonies<sup>14,31</sup>. Each microcolony acts as an independent community and may contain a variety of bacterial species<sup>31</sup>. Bacteria that are located in the center of the microcolony usually live in a strict anaerobic environment, while others at the periphery of the microcolony are exposed to a more aerobic environment<sup>22</sup>. Therefore, a biofilm is a dynamic structure that can provide a range of environments with respect to nutrient and oxygen concentrations and thus may successfully harbor a diverse bacterial population<sup>31</sup>. To sustain these bacterial populations, a series of fluid channels exist between microcolonies to provide nutrients and oxygen required for normal bacterial growth and to facilitate outward movement of bacterial metabolites, waste products, and enzymes<sup>14,32,38</sup>. Additionally, each bacterial microcolony uses chemical signals to create a primitive communication system within the biofilm, a perfect niche for bacterial propagation and existence<sup>33,33,34</sup>.

## Development of Dental Plaque

The growth and development of dental plaque occurs in a four-phase process: initial attachment, rapid growth, steady state and detachment to the planktonic phase<sup>32</sup>.



**Figure 1:** Schematic of biofilm formation.

### Initial Attachment

The initial attachment of bacteria commences after the formation of the salivary pellicle. The pellicle is a thin coating of salivary proteins that adhere to the tooth surface within minutes after tooth eruption or cleaning. The pellicle is composed of albumin, glycoproteins, acidic proline-rich proteins, mucins, cell debris, amylase, lysozyme and sialic acid<sup>32,38</sup>. The pellicle provides a sticky base to support further colonization and propagation of bacteria. Acidic phosphoproteins and proline-rich proteins that aid in colonization of bacteria on to the tooth surfaces<sup>33</sup> mediate the initial interaction between the pellicle and the bacteria. In addition to the presence of pellicle, other environmental cues that can influence biofilm formation include low pH, changes in

osmolarity, and oxygen. The early plaque forming bacteria or the initial colonizers are generally Gram-positive cocci, which primarily comprise streptococcal species<sup>32,33,34</sup>.

### **Rapid Growth Phase**

Once microorganisms have established a foothold on the tooth surface, they undergo a series of changes. Common adaptations that have been observed include the expression of large quantities of exopolysaccharides that may protect the biofilm and lead to biocide resistance<sup>32,33,34</sup>. The biofilm grows through the attachment of new bacteria through a process of coaggregation<sup>17,25,26</sup>. Coaggregation is driven by specific receptor-ligand interactions that allow new bacterial colonizers to adhere to the previously attached cells and results in increased complexity of the microbial community<sup>17,25,26</sup>. A detailed knowledge of these mechanisms of bacterial attachment and co-adhesion could highlight mechanisms that may be exploited to control the pattern of biofilm formation<sup>32,33,34,38</sup>. For example, analogs could be synthesized that block adhesin-receptor attachment or co-adhesion or alternatively, chemical modification of the colonizing surface could make them less conducive to microbial colonization.

### **Steady State Phase and Detachment**

As plaque matures in the subgingival pocket, the host mounts an inflammatory response to the microbial challenge and the flow of gingival crevicular fluid (GCF) is increased<sup>32,38</sup>. The GCF not only delivers components of host defense but also serves as a continuous source of glycoproteins and co-factors that provide nutrients for the growing

microorganisms<sup>38</sup>. In addition, bacterial microcolonies produce degradative enzymes such as endotoxins and lipoteichoic acid that promote an inflammatory response in the gingival tissue<sup>34,38</sup>. Furthermore, the inflammatory host response and increased secretion of GCF leads to a transient increase in the local pH. This increase in pH favors the growth of anaerobic bacteria such as *Prevotella intermedia* and *P. gingivalis*<sup>34,38</sup>. As gingivitis progresses to periodontitis, the microflora can become even more diverse<sup>34,38</sup>. Periodontitis results in tissue damage, which is manifested clinically as attachment loss. Tissue damage results from the activity of the subgingival microflora and indirectly from the release of lysosomal enzymes during phagocytosis or by the production of cytokines that stimulate resident connective tissue cells to release metalloproteinases.

Detachment to the planktonic phase can occur by a variety of active or passive processes. For example, some organisms may express enzymes that degrade the extracellular matrix leading to cell dispersion, while other organisms may reduce the expression of enzymes that are required for biosynthesis of the matrix. Portions of the mature biofilm may also simply slough off and colonize elsewhere.

### **Implication for the Etiology of Periodontal Diseases**

There are two main hypotheses that explain the role of plaque bacteria in disease<sup>19,20</sup>. First, the “Specific Plaque Hypothesis” proposes that out of the diverse species that exist in dental plaque, only specific species are actively involved in causing disease even if these species are present in low abundance<sup>11,19,20,31,30,39</sup>. Consistent with this, specific organisms such as *P. gingivalis*, *T. forsythia*, and *T. denticola* have all been strongly associated with adult periodontitis<sup>4,5,8,10,23,35</sup>. Furthermore, recent studies also suggest that *P. gingivalis* may play a pivotal role in disrupting host-microbe homeostasis

and function as a “keystone” pathogen even when present at low abundance in a complex multispecies biofilm<sup>28,29,30</sup>. These studies further indicate that by altering the host response, *P. gingivalis* induces changes in microbial populations in the biofilm leading to uncontrolled inflammation and tissue damage. However, the Specific Plaque Hypothesis cannot adequately explain the absence of the putative pathogens in some cases of disease nor the presence of these pathogenic organisms in healthy patients<sup>19</sup>. In contrast, the "Non-Specific Plaque Hypothesis" purports that many of the heterogeneous mixture of organisms in plaque could play a role in disease, and that disease is a result of the overall interaction of the plaque microflora with the host<sup>19</sup>. It is well established that plaque mediated diseases has multi factorial etiology and a variety of organisms are involved in its progression. Therefore, the specific plaque theory is puzzling, however it does demonstrates some specificity with respect to disease causing organisms. Consequently, a modified hypothesis was proposed which suggested that changes in environmental factors lead to a shift in the resident microflora resulting in microbial dysbiosis<sup>19</sup>. The occurrence of potentially pathogenic species as minor members of the resident plaque microflora would be consistent with this proposal<sup>19</sup>. In health, these organisms would be weakly competitive and mostly be suppressed by intermicrobial antagonism, so that they would comprise only a small percentage of the plaque microflora and would not be significant clinically<sup>19</sup>. Microbial specificity in disease would be due to the fact that the new environmental conditions would activate only a certain group of microorganisms. It is a basic tenet of microbial ecology that a major change to an ecosystem produces a corresponding disturbance to the stability of the resident microbial community<sup>19</sup>.

## **Significance of *Porphyromonas gingivalis* and *Streptococcus gordonii* Interaction in Dental Plaque Biofilm Formation**

Previous work suggests that the adherence of *P. gingivalis* to oral streptococci is an initial event that facilitates *P. gingivalis* colonization of the oral cavity<sup>8,9</sup>. Adherence is driven by a protein-protein interaction between the minor fimbrial antigen (Mfa1) of *P. gingivalis* and antigen I/II (AgI/II) of specific streptococcal species<sup>5,8,9,10,12</sup>. This interaction is mediated by a specific motif in AgI/II, designated BAR<sup>8,9</sup>. A synthetic peptide representing BAR potently inhibited the formation of *P. gingivalis*/*S. gordonii* biofilms in vitro (IC<sub>50</sub>=1.3μM)<sup>8,9,10</sup> and significantly reduced *P. gingivalis* virulence in mice that harbor *S. gordonii* when administered simultaneously with *P. gingivalis* infection<sup>9</sup>. These results suggest that BAR peptide blocks *P. gingivalis* colonization of the oral biofilm and may represent an effective therapy to limit recolonization of the oral cavity by *P. gingivalis* after professional prophylaxis. However, a limitation of this potential therapeutic approach is that BAR can only be transiently administered. In addition, while BAR potently inhibits the formation of two species biofilms, it is less effective in disrupting preformed biofilms or more complex communities, which required a higher concentration (i.e., IC<sub>50</sub>=3.6μM)<sup>18</sup> and/or prolonged exposure to BAR (i.e., > 60 minutes)<sup>10,7</sup>. Together, these data suggest that BAR is more effective inhibiting the initial association of *P. gingivalis* and streptococci than disrupting established complex biofilms<sup>8,10,18</sup>. This represents a potential limitation for developing the peptide as a therapeutic for clinical evaluation in humans. Therefore, the goal of this study was to

develop a method to deliver higher localized concentrations of BAR to the oral cavity to improve BAR effectiveness. Our hypothesis is that nanotechnology may be applied to develop novel non-toxic, poly(lactic-co-glycolic acid; PLGA) nanoparticle (NP) delivery vehicles that increase BAR effectiveness by promoting multivalent surface interactions of BAR with *P. gingivalis*.

### **Nano-sized Technology in Advanced Therapeutics**

In recent times, many therapeutic agents have been developed to treat or prevent dental caries and periodontal disease – the two major oral biofilm-associated infections<sup>2</sup>. Traditionally these therapeutic agents have been comprised of antimicrobials that are delivered to target tissues via oral, subcutaneous or local delivery routes<sup>40,27</sup>. When administered via oral doses, these agents are often destroyed either by enzymes in saliva or during intestinal transit resulting in decreased efficacy<sup>50,51</sup>. Moreover, uncontrolled levels of antimicrobials may lead to concentration spikes resulting in serious side effects and toxic reactions<sup>40,27</sup>. On the other hand, localized drug delivery vehicles including strips, gels and antimicrobial membranes have difficulty accessing the periodontal pockets and resisting recolonization by pathogens, rendering them only partially successful<sup>2</sup>. In contrast to these technologies, delivering antimicrobial molecules via NPs may circumvent many of the challenges mentioned above, thereby producing more effective therapeutics<sup>27</sup>.

NP drug delivery systems offer many advantages over conventional prophylaxes or therapeutics. One advantage of NPs is that their small size enables them to more effectively penetrate barriers and allow for drug accumulation at target sites, resulting in

enhanced treatment efficiency<sup>40</sup>. NPs have been developed using a variety of materials including metals, ceramics and polymers<sup>40,2,1</sup>. Among several biomaterials, particles made of colloidal gold, iron oxide crystals, hydroxyapatite and silver have been used as antimicrobial agents to prevent dental caries<sup>2,1</sup>. The proposed mechanism of these antibacterial metallic particles is believed to arise from an electrostatic attraction of positively-charged NPs with the negative charge of the bacterial cell membrane<sup>1</sup>. Furthermore, NPs have been investigated for a range of applications including incorporation into dentures, orthodontic adhesive materials and dental resin composites for preventing secondary caries<sup>2</sup>. Other novel systems based on silica have been investigated for anti-biofilm properties<sup>2</sup>. In particular, the use of nitric-oxide-releasing silica NPs to kill biofilm-based microbial cells has recently been investigated<sup>2</sup>. The rapid diffusion of NO may result in enhanced penetration of oral biofilm and thereby, improved anti-biofilm properties<sup>2</sup>. Although the development and the application of nanotechnology have shown immense promise, there have been considerable concerns regarding the potential toxicity associated with metallic NP accumulation in different tissues and organs<sup>1</sup>. To circumvent the challenge of metal cytotoxicity, polymeric NPs have been developed to provide safer and more durable options for drug delivery<sup>55</sup>. In addition, they offer biocompatibility and flexible tuning of physical properties to achieve desired dosages and drug release profiles<sup>27</sup>.

### **Polymeric Nanoparticles**

Synthetic and natural polymeric NPs have been extensively researched as potential vehicles for drug delivery<sup>49</sup>. Synthetic polymers have the advantage of high purity over natural polymers and may be less likely to evoke an immune response (i.e.,

less immunogenic)<sup>40,27</sup>. Among the variety of synthetic options, poly(lactic acid) (PLA), poly( $\epsilon$ -caprolactone) (PCL), polyethyleneimine, and poly(glycolic acid) (PGA) are extensively used in preventing oral biofilms because of their biodegradability and biocompatibility<sup>27</sup>. Among the different polymeric materials, poly(lactic-co-glycolic acid) (PLGA) has attracted considerable attention due to its FDA approval for human therapy<sup>27</sup>. Furthermore, PLGA NPs have well described formulations that can deliver a variety of agents, e.g. hydrophilic or hydrophobic small molecules or macromolecules<sup>27</sup>. Currently, PLGA NPs have been investigated for their use in bone loss in severe periodontitis<sup>2</sup>. Another interesting use of PLGA NPs is in photodynamic therapy, which is a novel alternative to conventional antimicrobials<sup>2</sup>. Photodynamic therapy works on the concept that a photosensitive agent, which absorbs light, can be preferentially incorporated into bacteria and subsequently activated by light. Activation leads to the generation of singlet oxygen and free radicals that are cytotoxic to bacterial cells<sup>2</sup>. For this, PLGA NPs are coupled with photosensitive methylene blue (MB)<sup>2</sup>. PLGA/MB NPs have proven to be effective against various Gram positive and Gram-negative bacteria associated with endodontic and periodontal infections<sup>2</sup>. Furthermore, dexamethasone/PLGA NPs have been extensively studied for their osteoblastic differentiation in periodontal disease<sup>2</sup>. In summary, PLGA NPs provide a biocompatible, non-immunogenic, biologically stable carrier that can encapsulate and/or present on its surface a wide range of biologically active molecules of therapeutic significance<sup>2,27</sup>. Even though additional studies are required to understand the behavior of particles in preventing oral infections, it is important to note that these polymeric NPs are a promising alternative to conventional antimicrobials<sup>27</sup>.

## CHAPTER 2

### HYPOTHESIS AND SPECIFIC AIMS

Therapeutic approaches that target specific periodontal pathogens or groups of organisms are lacking. Currently, treatment of periodontal disease involves the removal of plaque from the gingival pocket (with possible antibiotic treatment) and if necessary, gingival surgery to reduce pocket depth. To our knowledge, no therapeutic approach exists that promotes host-biofilm homeostasis by limiting pathogen colonization of the biofilm or recolonization after prophylaxis or treatment. To develop an approach that specifically targets pathogen interactions, this project builds upon our previous discovery of a peptide that specifically inhibits *P. gingivalis* colonization of the oral biofilm. We seek to develop peptide delivery *PLGA*-NPs that not only target *P. gingivalis*, but also deliver BAR to niches in the oral cavity where it will be most effective. We anticipate that these targeted NPs will deliver BAR at higher localized concentrations to specific niches in the oral cavity or microbiome. While tissue targeted NPs have been used against a variety of pathologies, their application and targeting to specific organisms and niches in the oral microbiome represents a novel approach to combat periodontal disease.

#### **Specific Research Hypothesis**

Surface-modified NPs will facilitate multivalent interactions between BAR and the minor fimbrial antigen leading to increased inhibition of *P. gingivalis* adherence to streptococci relative to equimolar amounts of free BAR peptide.

### **Specific Aims**

To compare the inhibitory potency of BAR-NPs with soluble BAR we will:

1. Synthesize PLGA NPs that are surface-modified with BAR peptide to facilitate multivalent interaction with *P. gingivalis*.
2. Quantify the density of BAR peptide on the NP surface to optimize the concentration of BAR surface modification.
3. Compare the efficacy of BAR-NPs with the molar equivalent of free BAR peptide using dual and three biofilm model systems.

CHAPTER 3  
MATERIALS AND METHODS

Peptide Synthesis

The BAR peptide used in this study, is shown in Table 1. The peptide is comprised of residues 1167 to 1193 of the SspB (Antigen I/II) protein sequence of *S. gordonii*<sup>16</sup>. The peptide containing a covalently attached biotin at its N-terminus was synthesized by BioSynthesis, Inc. (Lewisville, TX) and was obtained at more than 85% purity.

**Table 1:** Sequence of BAR peptide.

Peptide	Peptide Sequence
BAR	NH <sub>2</sub> -LEAAPK <u>K</u> VQDLLKKANITVKGAFQLFS-OH

To assess the level of BAR present on the NP surface, biotin-BAR was also synthesized that contained 6-carboxyfluorescein (Flc) covalently attached to the epsilon amine of the lysine residue underlined in Table 1 to generate BAR-Flc. For functional controls with free peptide, BAR without biotin or fluorophore was utilized.

### **Growth of Bacterial Strains**

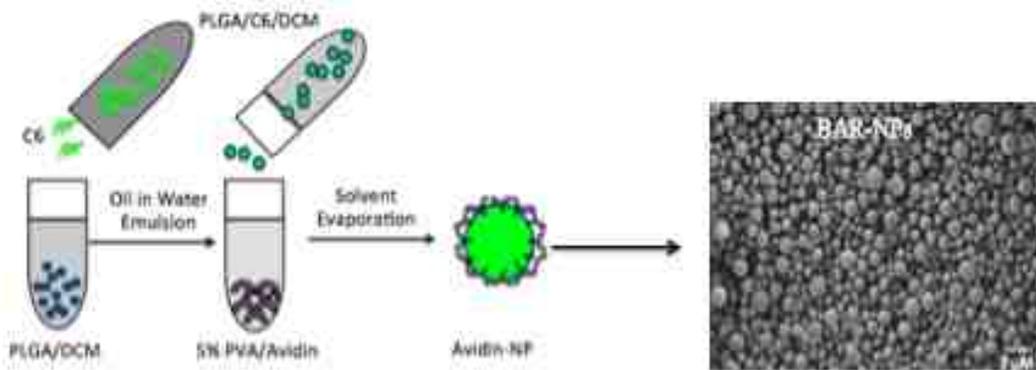
*P. gingivalis* strain ATCC 33277 was grown in Trypticase soy broth media (TSBY media) (Difco) supplemented with 0.5% (w/v) yeast extract, 1 µg/ml (final concentration) menadione, and 5 µg/ml (final concentration) hemin. Twenty milliliters of medium was reduced for 24 hr under anaerobic conditions consisting of 10% CO<sub>2</sub>, 10% H<sub>2</sub>, and 80% N<sub>2</sub>. Next, *P. gingivalis* was inoculated into the medium and grown for 48 hr at 37°C under anaerobic conditions. *S. gordonii* DL-1 was cultured aerobically without shaking in brain-heart infusion (BHI) broth supplemented with 1% yeast extract for 16 hr at 37°C.

### **Synthesis of Avidin-Palmitate Conjugates**

To obtain BAR-modified PLGA NPs, the NP surfaces were modified with avidin-palmitate to attach biotinylated BAR. Avidin-palmitate was conjugated as previously described by Fahmy and Saltzman. Briefly, 100 mg/8 ml solution of avidin was made in 2% (w/v) sodium deoxycholate (NaDC) in PBS and warmed to 37°C. 4.5 mg/2 ml solution of palmitic acid-NHS (PA-NHS, Sigma) was prepared in 2% (w/v) NaDC and sonicated until well-mixed. Two milliliters of the above made PA-NHS solution was added dropwise to the reaction vial containing avidin, and reacted overnight at 37°C. The following day, the reaction was dialyzed in 1200 mL of 0.15% (w/v) NaDC in PBS heated to 37°C using a 3500 molecular weight cut off (MWCO) dialysis tubing to remove free PA-NHS. After overnight dialysis at 37°C, complexed avidin-palmitate was transferred to a storage vial from the dialysis cassette and stored at 4°

## Nanoparticle Synthesis

Unmodified and surface-modified PLGA NPs, encapsulating the fluorescent dye Coumarin 6 (C6) for binding and internalization studies were synthesized and characterized as broadly depicted in Figure 2.



**Figure 2:** Overview of NP synthesis with an example of the resulting NP morphology analyzed with scanning electron microscopy (SEM). \*Scale bar = 1 μm.

## BAR-Modification of C6 NPs

C6 NPs were synthesized using an oil-in-water (o/w) single emulsion technique<sup>31</sup>. Briefly, C6 was encapsulated in 100-200 mg poly(lactic-co-glycolic acid) (PLGA) carboxyl-terminated polymer (0.55-0.75 dL/g, LACTEL<sup>®</sup>). C6 was dissolved in methylene chloride (DCM) overnight at a concentration of 15 μg C6 per mg of PLGA. In parallel, 200 mg PLGA crystals were dissolved in 2 ml of DCM overnight. The following day, the PLGA/DCM solution was vortexed while adding 200 μl of the prepared C6 DCM solution. The PLGA/DCM/C6 solution was sonicated to attain a uniform solution. Next, 2 ml of 5% (w/v) polyvinyl alcohol (PVA) solution was mixed with 2 ml of 10 mg/ml avidin-palmitate to obtain a well-mixed solution. To create the single emulsion, 2

mL PLGA/DCM/C6 solution was added dropwise to 4 ml PVA/avidin-palmitate under vortexing and subsequent sonication. The residual DCM was evaporated by adding the NP solution to 50 mL of 0.3% PVA for 3 hr while mixing. After solvent evaporation, the 50 ml NP solution was transferred to tubes and centrifuged at 13,000 rpm at 4°C to wash NPs, prior to BAR-peptide conjugation. The supernatant was discarded and the pelleted NPs were resuspended in 9 ml of diH<sub>2</sub>O. The resuspended NPs were incubated for 30 min on a benchtop rotator with biotinylated BAR peptide at a molar ratio of 3:1 BAR:avidin (18.5 nmol/mg) in PBS. After conjugation, the NPs were centrifuged at 13,000 rpm and the supernatant was discarded. The NPs were resuspended in 20 ml diH<sub>2</sub>O and centrifuged twice to remove any remaining unbound BAR peptide. After the three washes, the NPs were suspended in 9 ml of diH<sub>2</sub>O, transferred to a 10 ml cryotube, frozen in -80°C for 3 hr and subsequently lyophilized. All NPs were stored at -20°C after synthesis. Unmodified C6 NPs were prepared similarly, however 5% (v/v) PVA alone was added instead of PVA/avidin-palmitate solution.

### **Nanoparticle Characterization**

Particle size and morphology were determined using scanning electron microscopy (SEM). Dry NPs were mounted on carbon tape and sputter coated with gold under vacuum. Average particle diameter and size distribution were determined from SEM images of at least 400 particles per batch using image analysis software (ImageJ, National Institutes of Health). Zeta potential and dynamic light scattering (DLS) were measured with a Zetasizer Nano ZS (Malvern) in diH<sub>2</sub>O to determine particle charge and hydrated diameter. NPs with zeta potential values ranging from +25 mV to -25 mV

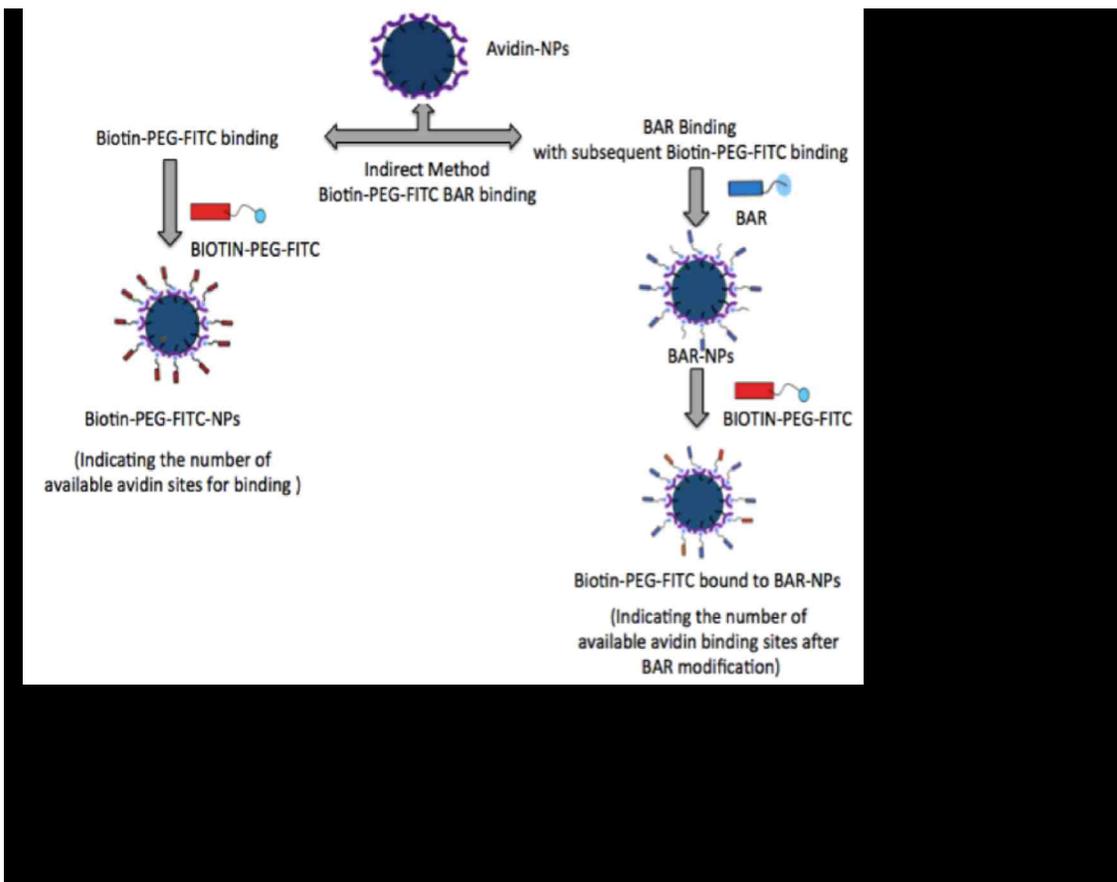
typically have high degrees of stability, indicating less potential for NP aggregation.

### **Functional Characterization**

As described below, indirect and direct methods were used to quantify the density of BAR peptide on the NP surface.

1. Indirect: The binding of biotin-PEG-FITC to both avidin-NPs and BAR-NPs was measured (Figure 3).
2. Direct: The binding of fluorescently-labeled BAR peptide to avidin-NPs was measured (Figure 4).

### **Indirect Characterization: Biotin-PEG-FITC Reaction**

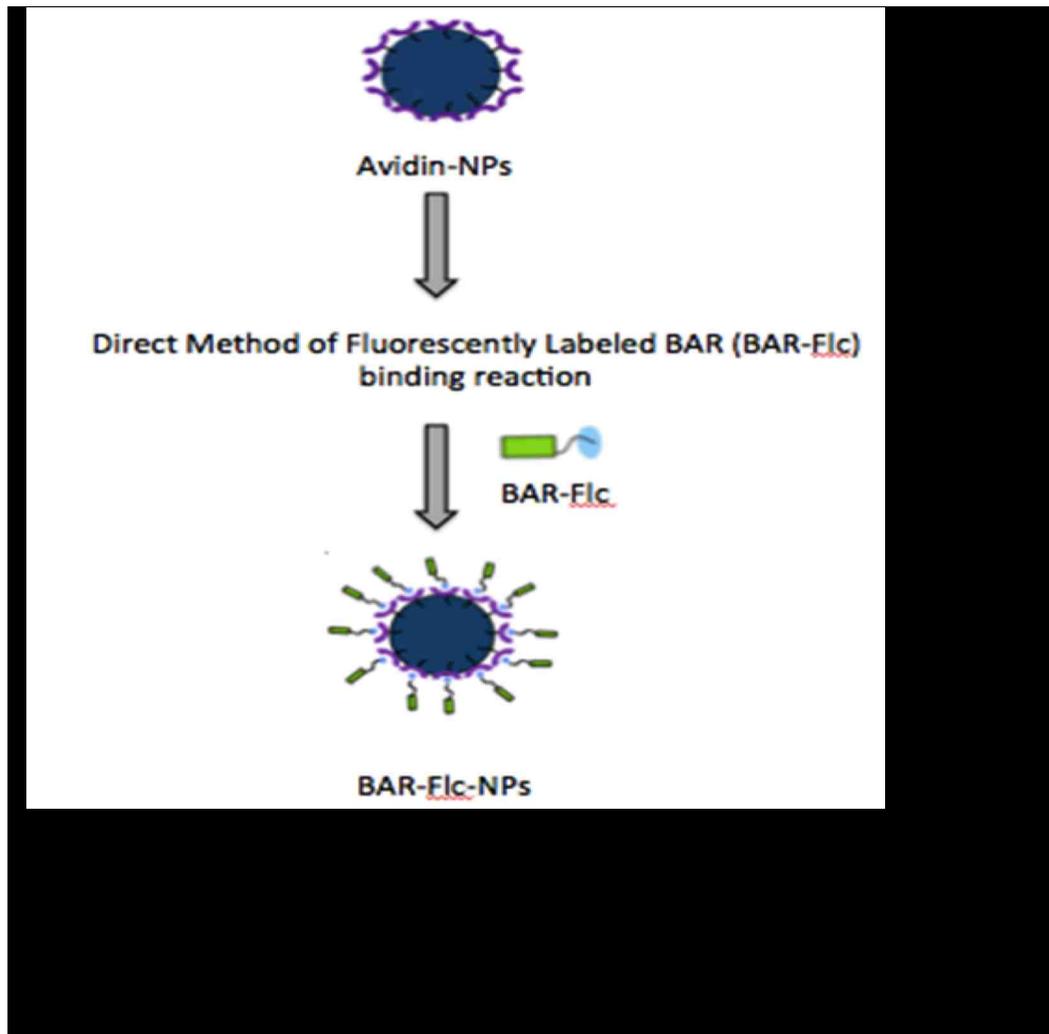


Avidin-NPs (20 mg) were synthesized and aliquoted to a 15 ml tube. These NP swere reacted with 18.5 nmol/mg of biotin-PEG-FITC for 1 hr on a rocker platform in the dark. PEG3400 was used to quantify binding indirectly since it is similar in molecular weight to biotinylated BAR (3400 vs. 3329 Daltons). The concentration of biotin-PEG-FITC used in these reactions (i.e., 18.5 nmol/mg) was determined by first calculating the total number of available biotin binding sites on surface-modified avidin, with the assumption that each avidin molecule has 2 available biotin binding sites, and then adding biotin-PEG-FITC at a molar ratio of 3:1 biotin-PEG-FITC: biotin binding sites. After conjugation, the NPs were washed twice with diH<sub>2</sub>O by centrifugation at 15,000 rpm. After synthesis, the washed particles were frozen, lyophilized and stored at -20°C. The following day, the biotin-PEG-FITC labeled NPs were suspended in freshly prepared 1X PBS (10 mM NaH<sub>2</sub>PO<sub>4</sub>, 137 mM NaCl, and 2.7 mM KCl, pH 7.4) at 1 mg/mL and subsequently diluted 1:2, 1:5 and 1:10-fold in PBS. Samples (100 µl each) were then transferred into a microtiter plate in triplicate.

A standard curve of biotin-PEG-FITC was obtained by making serial dilutions of a 1 mg/ml biotin-PEG-FITC stock solution to generate a concentration range of 0.002 to 5 µg/ml biotin-PEG-FITC. The diluted NP samples and standards were measured for fluorescence at 488nm. The amount of bound biotin-PEG was determined from the standard curve generated with biotin-PEG-FITC. This identified the density of biotin-PEG-FITC on the NP surface resulting from a given set of reaction conditions and also identified the concentration of biotin-PEG-FITC required to saturate the avidin present on the NP surface. Next, another aliquot of avidin-modified NPs was conjugated with biotinylated BAR and the resulting BAR-NPs were subsequently incubated with a

saturating concentration of biotin-PEG-FITC (i.e., 18.5 nmol of biotin-PEG-FITC per 1 mg NPs). NP-associated fluorescence was determined as above and the amount of bound biotin-PEG-FITC was determined from the standard curve. Total BAR modification was calculated with the following equation: [biotin-PEG-FITC associated with avidin-NPs] - [biotin-PEG-FITC associated with BAR-modified NPs]. This difference represents the amount of BAR conjugated to the NP surface.

**Direct Characterization: Binding of Fluorescently-Labeled BAR to Avidin-NPs**



The second approach that was used to quantify BAR binding was to directly measure BAR binding to avidin-NPs. This was accomplished using biotinylated BAR in which an internal lysine was labeled with 6-carboxyfluorescein Flc, (see Table 1). Avidin-NPs (5 mg) were aliquoted to eppendorf tubes and mixed with increasing concentrations (3-, 6-, 9-, 18- fold molar excess of BAR) (18.5 – 111.2 nmol/mg NP) of fluorescently labeled BAR (BAR-Flc) for 45 min on a rocker platform in the dark. After conjugation, the NPs were washed twice with diH<sub>2</sub>O after centrifugation at 15,000 rpm. The washed samples were frozen, lyophilized and stored at -20°C after synthesis. On day 2, NPs from each eppendorf tube were aliquoted and suspended in 1X PBS to attain suspensions of 1 mg NP/ml. The resulting samples were transferred to a microtiter plate in triplicate. After conjugation with BAR-Flc, total NP-associated fluorescence was calculated from a standard curve obtained from known BAR-Flc concentrations. Both the indirect and direct approaches described above allowed us to quantify the amount of BAR peptide bound to the NP surface and enabled us to optimize the synthesis and conjugation conditions to obtain maximal binding of BAR to the NP surface. Surface-modification using avidin-biotin linkages represent an established and efficient method to conjugate our novel peptide to the NP surface<sup>56</sup>.

### ***P. gingivalis* Binding Assay**

The adherence of BAR-NPs to *P. gingivalis* was assayed using BAR-modified NPs that encapsulated the fluorescent probe C6. *P. gingivalis* was cultured as previously described and to establish a uniform cell concentration across all samples, *P. gingivalis* suspensions were adjusted to a final optical density of 0.4. Subsequently, a 1 ml aliquot

of *P. gingivalis* cells was transferred into eppendorf tubes and mixed with increasing concentrations of BAR-modified C6 encapsulated NPs (1 µg/ml, 2.5 µg/ml, 5 µg/ml, and 10 µg/ml) for 45 - 60 mins on a rocker platform in the dark. Negative controls for this experiment consisted of: 1) *P. gingivalis* incubated with unmodified C6 NPs and 2) BAR-modified C6 NPs incubated in buffer without *P. gingivalis* to evaluate nonspecific binding. After incubation, the samples were centrifuged at 5600 rpm for 5 min and the supernatant was discarded to remove the unbound particles. The remaining cells were resuspended in 1X PBS. One hundred microliters of each sample were transferred to a microtiter plate and the cell bound fluorescence was measured at 488 nm.

### **Dual Species Biofilm**

Cultures of *P. gingivalis* and *S. gordonii* were obtained as previously described. *S. gordonii* DL-1 cells were harvested by centrifuging a 12 ml culture of *S. gordonii* at 5600 rpm for 5 min. The supernatant was discarded and the cell pellet was resuspended in 1 ml of 1X PBS. *S. gordonii* was labeled with 20 µl of 10 mM hexidium iodide (5 mM, Molecular Probes, Eugene, OR) for 15 min at room temperature on a rocker platform protected from light. After incubation the labeled samples were centrifuged at 5600 rpm for 5 min, the supernatant was discarded, and the cells were resuspended in 1 ml of 1X PBS. Following this, the optical density (O.D) was measured at 600 nm from ten-fold diluted cultures of *S. gordonii* to determine cell count.

For all experiments, the optical density of *S. gordonii* cells was adjusted to 0.8 for uniformity of the *S. gordonii* cell amounts in each well. After adjusting the optical density, 1 ml of *S. gordonii* cells was added to a 12 well culture plate containing a

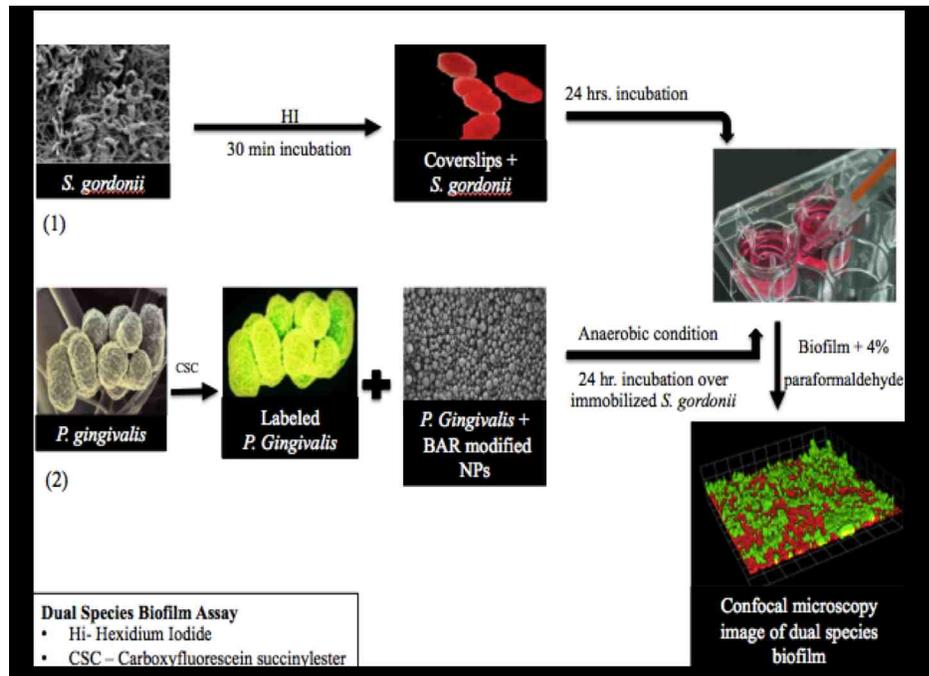
sterilized micro-coverslip in each well. The 12 well cell culture plate was wrapped in aluminum foil to protect the labeled cells from light and placed on a rocker platform in the anaerobic chamber for 24 hr.

*P. gingivalis* cultures used for biofilm formation were optimized using a similar approach. Briefly, 12 ml of *P. gingivalis* cells were centrifuged for 5 min at 5600 rpm. The supernatant was discarded and the cell pellet was resuspended in 1 ml of pre-reduced 1X PBS. *P. gingivalis* cells were labeled with 20  $\mu$ l of carboxyfluorescein-succinylester (4 mg/ml, Molecular Probes). Cells were incubated with the fluorescent dye for 30 min and protected from light. Following incubation, cells were centrifuged at 10000 rpm for 1 min and the supernatant was discarded to remove the unbound fluorescent dye. The pelleted cells were resuspended in 1ml of pre-reduced 1X PBS.

Previous experiments showed that the optimal inoculum for *P. gingivalis* was a cell suspension that was adjusted to an optical density of 0.4. For biofilm inhibition assays using BAR-NPs, the initial optical density (600 nm) was adjusted to 0.8 and the cell suspension was subsequently diluted with an equal volume of the BAR-NP suspension to generate a final O.D. 600 nm of 0.4. For biofilm inhibition experiments, BAR-NPs or soluble BAR peptide was pre-incubated with labeled *P. gingivalis* cells at peptide concentrations ranging from 0 to 10  $\mu$ g/ml at 25°C for 30 min before transferring to the appropriate wells. The 12 well cell culture plate was covered with aluminum foil and incubated for 18-24 hr in an anaerobic chamber.

Following incubation, the supernatant was removed from the wells of the 12 well cell culture plate and the cells were washed with pre-reduced 1X PBS to remove non-adherent bacterial cells. The cells were subsequently fixed with 4% (w/v) using

paraformaldehyde, excess paraformaldehyde was removed, and the cells were washed with pre-reduced 1X PBS. The coverslip was then mounted on to a glass slide using Prolong Gold anti-fade reagent and viewed using confocal laser scanning microscopy.



### **Confocal Microscope**

*P. gingivalis*-*S. gordonii* biofilms were visualized using an Olympus Fluoview 500 confocal laser scanning microscope (Olympus, Pittsburgh, PA). The slides were viewed using an argon laser for visualization of FITC-labeled *P. gingivalis* and the HeNe-G laser to visualize hexidium iodide- labeled streptococci. *P. gingivalis* binding was determined from 30 to 60 randomly chosen frames using FluoView Software. Z-stack images of the biofilms were obtained using a z-step size of 0.7  $\mu\text{m}$  and images were analyzed with the Volocity image analysis software.

### **Image Analysis**

After obtaining the images from confocal microscopy, the resulting z-stack images were processed and reconstructed into 3D images using the Volocity software. Images were imported into Volocity as multiple Tiff-files. Uniform filters were used to remove noise from the images and were further analyzed to quantify the extent of *P. gingivalis* binding. The image brightness and contrast was adjusted equally for all frames, and a snapshot of the image was captured. Next, the ratio of green to red fluorescence was determined. Each peptide concentration was analyzed in triplicate and 3 independent frames were measured for each well. The mean and variation (SD) between samples was determined using ANOVA. The variation was considered statistically significant when  $P < 0.05$ .

## CHAPTER 4

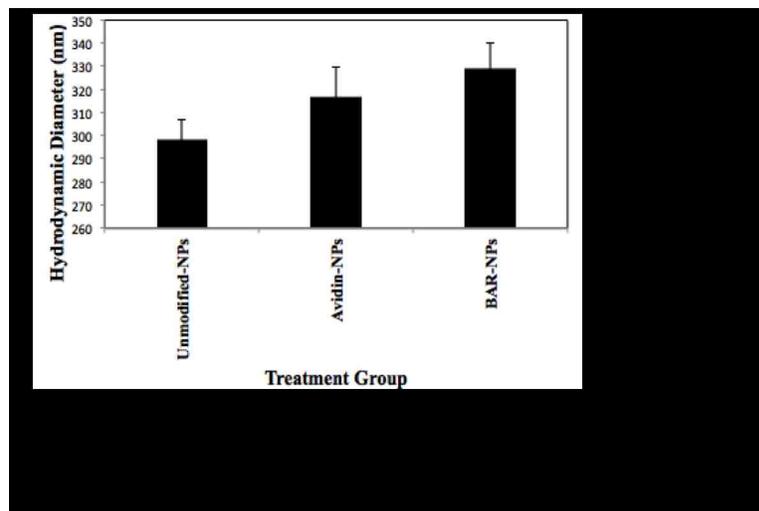
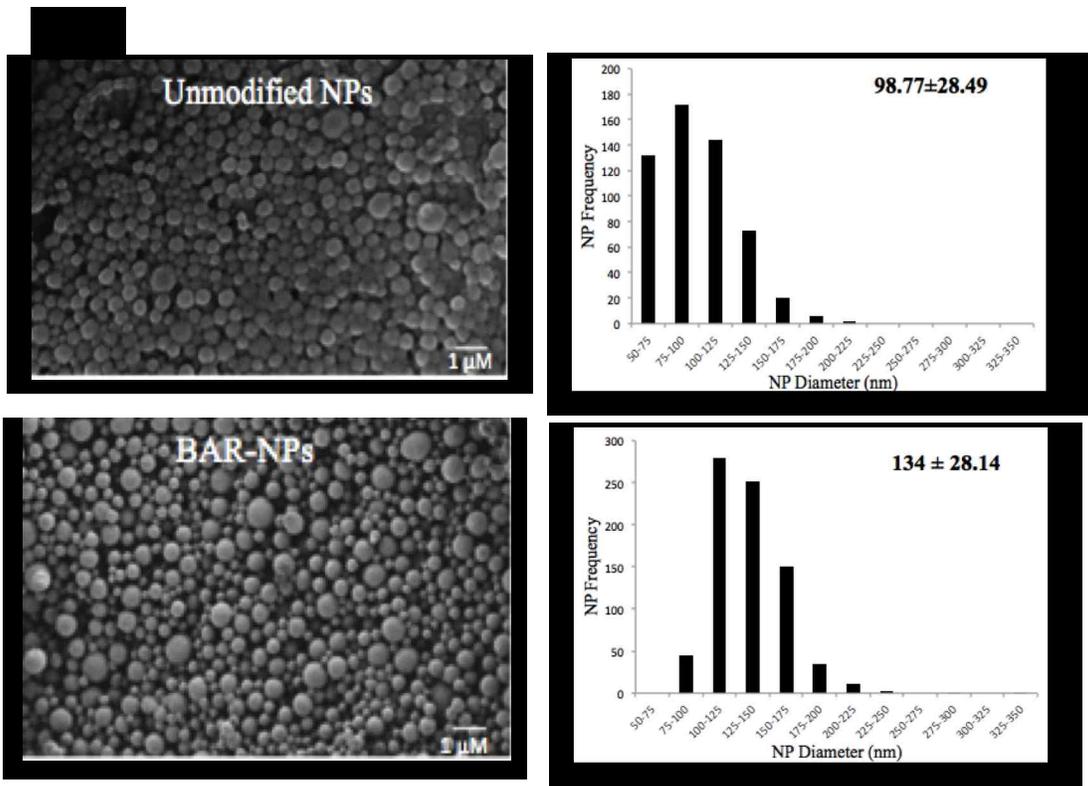
### RESULTS

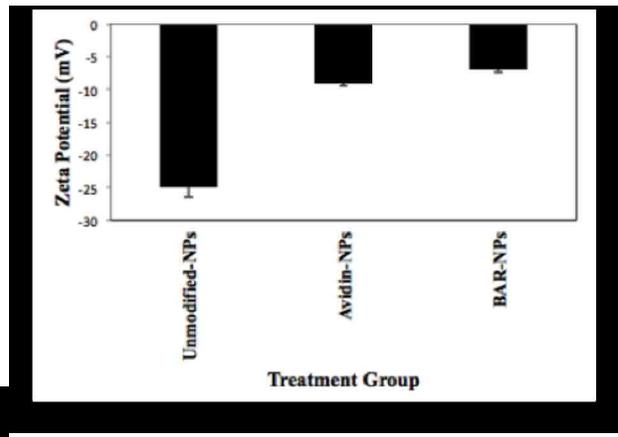
#### **Nanoparticle Synthesis and Characterization**

Previous studies have demonstrated the utility of coupling peptides to NP surfaces via avidin-biotin ligands (Av-ligand)<sup>41</sup>. In this study both the unmodified and BAR-NPs led to NPs of comparable size (Figure 6A). Analysis of SEM images shows the average NP diameters of  $98\pm 28$  and  $134\pm 28$  nm for unmodified and BAR-NPs, respectively. As expected, the presence of BAR on the NP surface did not significantly change the size of the NPs ( $P>0.05$ ). Furthermore, no change was seen in the characteristic texture and morphology after surface conjugation, relative to unmodified NPs. NP surface charge was measured by zeta potential, and DLS was used to measure the hydrodynamic diameter (Figure 6B). Average hydrodynamic diameters determined via DLS were  $298\pm 13$  nm and  $329\pm 10$  nm for the unmodified and BAR-NPs, respectively. As expected the diameters measured for hydrated NPs using DLS were slightly higher than the diameters of unhydrated NPs analyzed with SEM.

NP surface charge and hydrodynamic diameter were used to predict the long-term stability and surface-modification of the NPs. Zeta potential values were measured for NPs with avidin and BAR surface modification (Figure 6C). Unmodified NPs exhibited a negative charge of -25 mV. Addition of avidin to the NPs produced more positive zeta

potentials, which correlated with increased avidin density on the NP surface. When BAR was added to avidin-NPs, the zeta potential was slightly, but not significantly more positively charged, correlating with increased ligand conjugation. This is consistent with the net positive charge of BAR. Furthermore, there was a significant difference in zeta potential between the unmodified and avidin-NP groups and unmodified and BAR-NP groups ( $P < 0.01$ ). There was no significant difference between avidin-NPs and BAR-NPs.





The surface charge on unmodified and BAR-NPs was statistically significant ( $P < 0.01$ )

### **Surface Modification Efficacy and Functionality of PLGA-NPs**

To determine and optimize the amount of BAR peptide incorporated on the surface of the PLGA NPs, we utilized two different detection methods, an indirect method (biotin-PEG-FITC binding reaction) and a direct method (fluorescently-labeled BAR binding). The results from both the direct and indirect assays allowed us to optimize the synthesis and conjugation conditions to obtain maximal binding of BAR to the NP surface.

### **Quantification of the Total Biotin Binding Sites.**

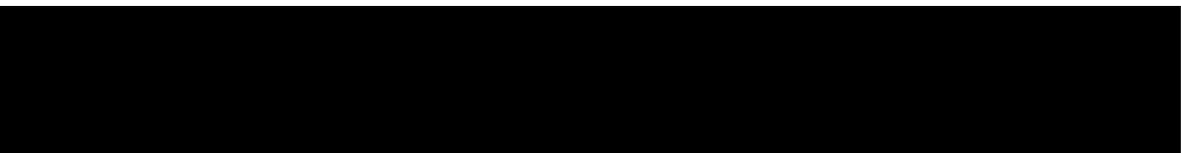
The incorporation of avidin on avidin-NPs was determined using the microBCA assay. The estimate of the number of available biotin binding sites was important for subsequent BAR modification. The microBCA indicated that 3.1 nmol/mg of avidin was

present on the surface per milligram NPs which was similar to the amount of avidin added to the synthetic reaction. This indicates that 100% of the input avidin (3.0 nmol/mg) was incorporated on the NP surface. Next the amount of avidin was converted into molecules of avidin per NP. This conversion indicated that 3940 molecules of avidin were present per NP. Although avidin has 4 biotin binding sites, we assumed that each molecule would only have 2 accessible biotin binding sites and the remaining 2 sites would be inaccessible due to steric hindrance. Hence, we calculate that 3.1 nmol/mg (3940 molecules/NP) of avidin would bind 6.2 nmol/mg (7880 molecules/NP) of BAR.

### **Indirect (Biotin-PEG-FITC Binding Experiment)**

In this experiment, we compared the fluorescence of avidin-NPs and BAR-NPs that were both treated with biotin-PEG-FITC to determine the number of available biotin binding sites before and after conjugation with biotinylated BAR. Biotin-PEG-FITC is comprised of PEG with a molecular weight of 3400 to closely match the molecular weight of BAR (3326 Da). Biotin-PEG-FITC was conjugated with both avidin-NPs and BAR-NPs at a ratio of 3:1 biotin-PEG-FITC: biotin-binding sites (18.5 nmol/mg biotin-PEG-FITC). Fluorescence of the resulting NPs was measured in triplicate and the mean fluorescence was quantified. The fluorescence values obtained were converted to an amount of PEG-FITC using a standard curve derived from increasing concentrations of biotin-PEG-FITC. Subtracting the level of biotin-PEG-FITC incorporated into BAR-NPs from the amount incorporated into avidin-NPs using Equation 1 allowed us to indirectly determine the number of BAR peptides present on the surface of BAR-NPs. Table 2 shows the number of biotin-PEG-FITC molecules per NP with the respective surface

modification. As expected, we found the surface density of biotin-PEG-FITC on BAR-NPs to be significantly less than biotin-PEG-FITC bound to avidin-NPs. Using a 3-fold (3:1) molar excess of biotin to avidin, 4.05 nmol/mg of biotin-PEG-FITC (5170 molecules/NP) was bound to avidin-NPs occupying 65 percent of the total biotin binding sites on the avidin-NP surface (Table 2). In contrast, when avidin-NPs were first conjugated with biotin-BAR and reacted biotin-PEG-FITC, 0.12 nmol/mg of biotin-PEG-FITC (149 molecules/NP) was incorporated on the surface of the BAR-NPs, occupying only 2% of the biotin binding sites, suggesting that 98% of the available biotin binding sites on avidin-NPs were occupied by biotin-BAR after conjugation (Table 2).

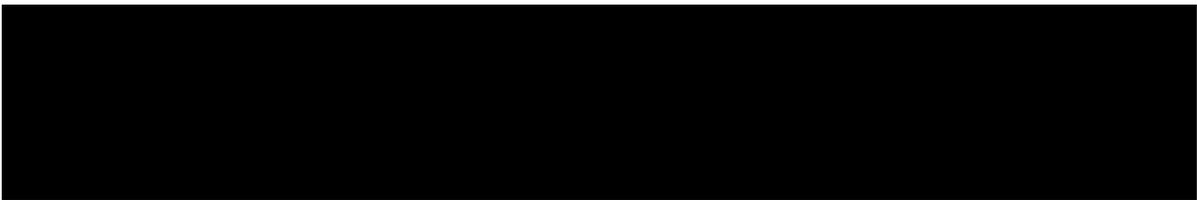


Sample	No. of Molecules of Avidin per NP Obtained from microBCA	# Avidin Binding Sites per NP Available for PEG-FITC Binding	# Biotin-PEG-FITC molecules/NP	% Biotin-PEG-FITC incorporation
Avidin-NPs	3940	7880	5170	65
BAR-NPs	3940	7880	149	2

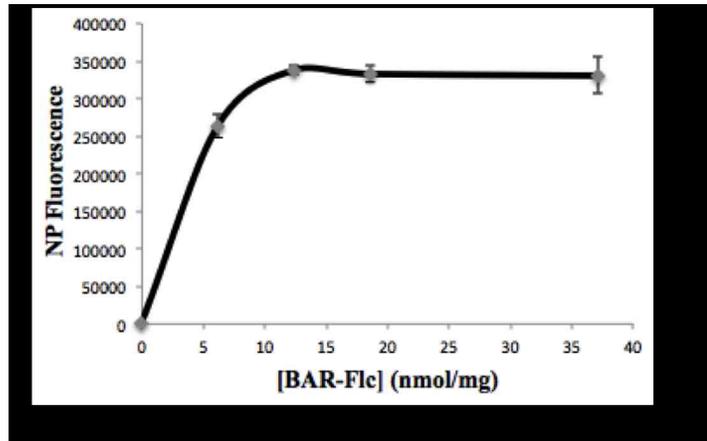
### **Direct (Fluorescently Labeled BAR Binding Experiment)**

To more directly determine the level of BAR incorporated after conjugation of avidin-NPs, we titrated avidin-NPs with 3-, 6-, 9- and 18- fold molar excess (18.5 – 111.2 nmol/mg) of fluorescently-labeled BAR (BAR-FIc). NPs were reacted with concentrations higher than 18.5 nmol/mg as the 3-fold excess used in indirect binding experiment indicated that higher concentration was needed for saturating the available avidin binding sites. NPs were incubated with BAR-FIc for 1 hr, washed, lyophilized, and

fluorescence was quantified as previously described. The incorporation of BAR-Flc on avidin-NPs was directly related to concentration of BAR-Flc added. As shown in Figure 8, we observed that saturation of BAR-Flc binding occurred with an input concentration of 37.1 nmol/mg (6- fold molar excess of calculated biotin binding sites) indicating that at this input concentration, all of the available biotin sites were bound with BAR-Flc. Mean fluorescence values did not significantly increase when NPs were conjugated with higher concentrations of BAR-Flc (Figure 8). Using a 3-fold (3:1) molar excess of BAR to avidin, 3.85 nmol/mg of BAR-Flc (4910 molecules/NP) was bound to avidin-NPs occupying 62.3% of the total biotin binding sites on the avidin-NP surface (Table 3). At the saturation concentration of 37.1 nmol/mg (6 fold molar excess of calculated biotin binding sites), 7.42 nmol/mg of BAR-Flc (9460 molecules/NP) was incorporated on the surface of the avidin-NPs, occupying 100% of the biotin binding sites. Furthermore, BAR-flc binding did not significantly increase when NPs were conjugated with higher concentration of BAR-Flc (55.6 - 111.2 nmol/mg)

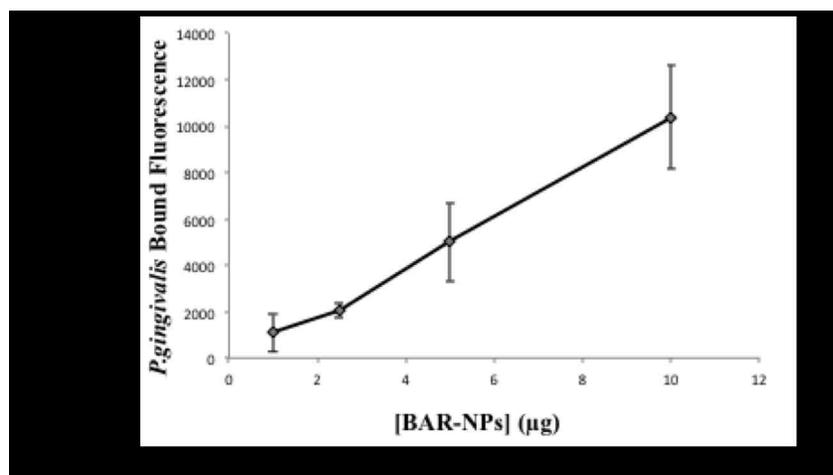


BAR-Flc Input Concentration	No. of Molecules of Avidin per NP obtained from microBCA	# Avidin binding sites per NP available for BAR-Flc Binding	# BAR-Flc molecules/NP	% BAR-Flc incorporation
18.5 nmol/mg (3:1)	3940	7880	4910	62.9
37.2 nmol/mg (6:1)	3940	7880	9460	100*
55.62 nmol/mg (9:1)	3940	7880	9310	100*
111.2 nmol/mg (18:1)	3940	7880	9360	100*



**Figure 7:** Saturation curve of BAR-Flc. Avidin-NPs were reacted with a 3-, 6-, 9-, 18-fold molar excess of BAR-Flc (18.5 – 111.2 nmol/mg NP) and the NP bound Fluorescence was determined and plotted.

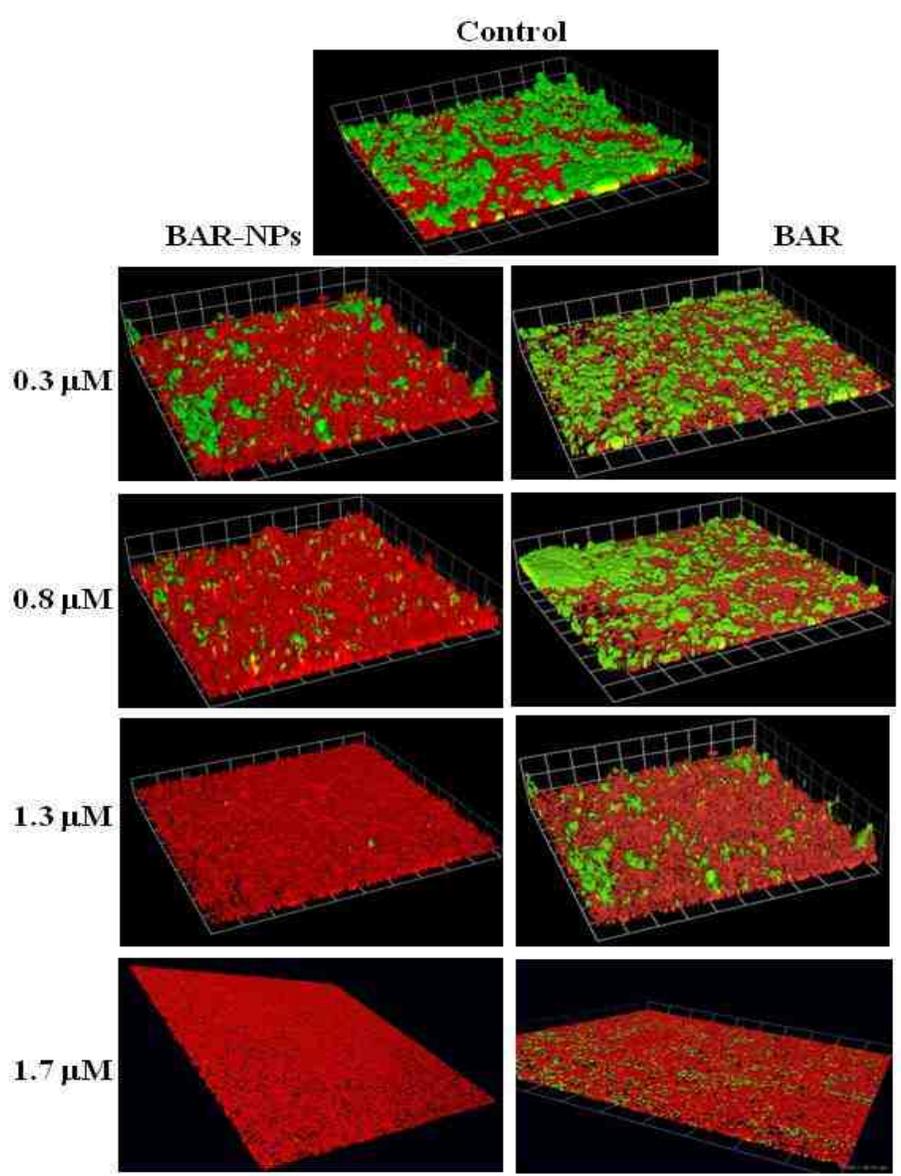
To determine if BAR-NPs were functional, we evaluated BAR-NP binding to *P. gingivalis*. BAR-NPs encapsulating the fluorophore C6 were incubated with *P. gingivalis* cells and cell-bound fluorescence was measured. In these experiments, the BAR-NP concentration was determined using total NP mass. As shown in Fig. 9, BAR-NPs bound to *P. gingivalis* cells in a dose-dependent manner. These results demonstrated proof-of-concept that uniformly sized BAR-NPs interact with *P. gingivalis* in a dose-dependent manner



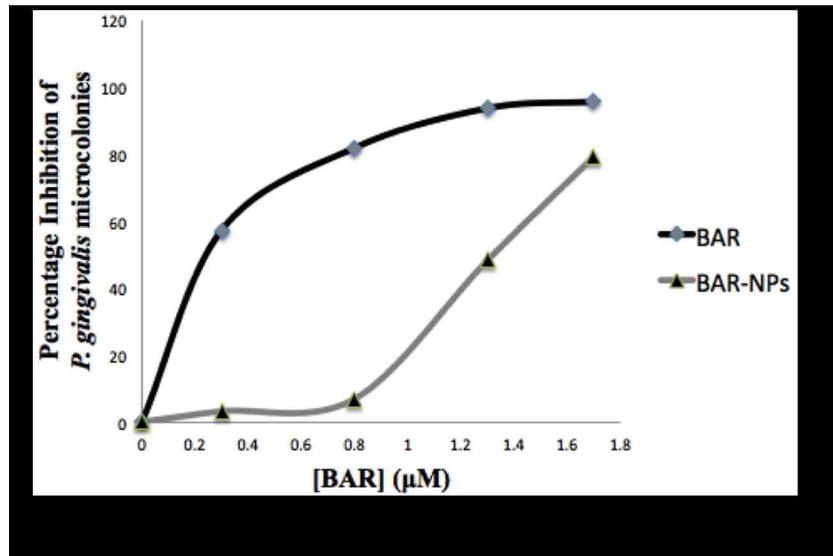
### **BAR Inhibits Formation of *P. gingivalis* Biofilms**

To determine if BAR-NPs competitively inhibit *P. gingivalis* adherence to streptococcal cells and prevent biofilm development, *P. gingivalis* biofilms were formed on immobilized streptococci in the presence of increasing concentrations of BAR-NPs for 24 hr. Previous studies showed that soluble BAR had an IC<sub>50</sub> (50% inhibitory concentration) of 1.3  $\mu$ M. Therefore, in these experiments, the amount of BAR on the surface of BAR-NPs was calculated using the direct binding results and sufficient amounts of NPs to deliver BAR peptide concentrations ranging from 0.3 to 1.7  $\mu$ M were tested and compared with similar concentrations of free soluble BAR.

*P. gingivalis* adherence to the immobilized streptococci was visualized using confocal scanning microscopy and the ratio of green (*P. gingivalis*) and red (*S. gordonii*) fluorescence was quantified using Volocity image analysis software. For control reactions, *P. gingivalis* was incubated with streptococci in the presence of buffer alone. The representative images of biofilms formed in the presence of BAR-NPs or soluble BAR are shown in Figure 10. As summarized in Table 3, BAR-NPs exhibited dose dependent inhibition of biofilm formation with the ratio of green to red fluorescence being significantly reduced ( $P < 0.01$ ) at all concentrations. The striking result was that BAR-NPs more potently inhibit *P. gingivalis* adherence than soluble BAR.



	Control	1.7 $\mu\text{M}$	1.3 $\mu\text{M}$	0.8 $\mu\text{M}$	0.3 $\mu\text{M}$
BAR peptide	0 %	79.3 %	50 %	6.9 %	3.3 %
BAR-NPs	0 %	95.7 %	93.7 %	81.9 %	57.3 %



These results show that NPs surface-modified with BAR peptide more potently inhibit *P. gingivalis* adherence to *S. gordonii* ( $IC_{50} \sim 0.29 \mu\text{M}$ ) than soluble ( $IC_{50} = 1.3 \mu\text{M}$ ), indicating that BAR-NPs are approximately 4.5 times more potent than soluble BAR. This suggests that BAR-NPs may promote multivalent interaction with *P. gingivalis* and that surface modified NPs may represent a viable mechanism to deliver higher localized concentrations of BAR peptide to the biofilm. Together, the results

provide proof-of-principle that targeted antimicrobial NPs can be utilized to control the complex biofilm associated with periodontal disease.

## CHAPTER 5

### DISCUSSION

The human oral cavity presents a hostile environment to microorganisms as a result of the constant flow of saliva that contains numerous antimicrobial agents<sup>11</sup>. The early colonizers protect themselves from these conditions by forming multispecies biofilms with other resident organisms<sup>11</sup>. The periodontal pathogen *P. gingivalis* faces different challenges in colonizing the oral cavity since it is an obligate anaerobe that is acid-sensitive and requires hemin as an essential growth factor<sup>11</sup>. Therefore, its primary niche is the subgingival pocket but before establishing itself in that niche, it must first survive in relatively aerobic supragingival environment<sup>11,23,24</sup>. To accomplish this, *P. gingivalis* interacts with the primary colonizer *S. gordonii* that provides a physiologically compatible local environment for *P. gingivalis*<sup>11</sup>. Since this interaction is one of the initial events that leads to *P. gingivalis* colonization of the oral cavity, it represents an ideal target for therapeutic intervention to limit *P. gingivalis* colonization and potentially reduce adult periodontitis<sup>11,22,23</sup>. Previous studies have been successful identifying the mechanisms of this interaction and adherence between *P. gingivalis* and *S. gordonii*<sup>11,23,24</sup>. It was found that the Mfa1 of *P. gingivalis* interacted with SspB of *S. gordonii*. Furthermore, *P. gingivalis* showed binding specificity with streptococcus gordonii and it did not adhere to Streptococcus mutans, which expressed SpaP, a highly conserved homolog of SspB. These studies led to the development of BAR peptide,

which is derived from the antigen I/II protein of *S. gordonii* and functions as a potent inhibitor of *P. gingivalis* adherence to *S. gordonii*. Corresponding a peptide derived from SpaP of *S. gordonii* mutants showed that it did not interact with Mfa1 of *P. gingivalis*. In addition, BAR significantly reduced *P. gingivalis* virulence in mice that harbor *S. gordonii* when administered simultaneously with *P. gingivalis* infection<sup>11,23</sup>. However, although BAR potentially inhibits the formation of two species biofilms, it is less effective in disrupting established biofilms or more complex biofilms, requiring higher concentrations and prolonged exposure to be effective. In this study, it was hypothesized that targeted nanoparticles comprised of an FDA-approved polymer, PLGA, and surface modified with BAR may enhance the potency of the peptide via two mechanisms: 1) by delivering BAR at higher localized concentration to *P. gingivalis* and 2) by promoting a multivalent binding interface to increase the avidity of BAR with *P. gingivalis*.

In this study a reproducible and rapid preparation method was developed to synthesize unmodified and BAR-NPs. Previous studies have demonstrated that avidin-biotin-ligand conjugation provides one of the strongest non-covalent bonds, while offering a flexible, tunable, and efficient method to conjugate and alter ligand density on the NP surface<sup>41</sup>. The synthetic process that was developed resulted in the production of spherical unmodified and BAR-modified NPs with a narrow particle size distribution (size about 100-134 nm). Additionally, we observed a negative surface charge for unmodified NPs but a slightly positive charge for BAR-NPs. This disparity of charge can be explained by the carboxyl groups of PLGA for unmodified NPs and the presence of cationic molecules, i.e., avidin and BAR on the surface of modified NPs<sup>41</sup>. Furthermore, the zeta-potential values for both unmodified (-25 mV) and BAR-NPs (-10 mV) are in

agreement with other unmodified and avidin-NP studies, where, unmodified PLGA NPs typically have a negative surface charge and avidin-modified NPs display a more positive surface charge. The statistically significant ( $P < 0.01$ ) surface charge that we observed between unmodified-NPs and BAR-NPs was attributed to successful conjugation with the positively-charged BAR peptide. For biological experiments, this positive zeta potential may also be beneficial as the positive NP surface charge might facilitate the interaction of NPs with *P. gingivalis* by promoting electrostatic attractions with the negative moieties on the bacterial cell membrane.

To design a NP formulation with maximal levels of BAR peptide, it was important to first quantify the number of avidin molecules present on the NP surface and available for subsequent BAR conjugation. To estimate the number of molecules of avidin per NP, we used the microBCA assay to confirm 100% incorporation of the input avidin to the NP surface. Although under these conditions, we were able to achieve virtually 100% incorporation of avidin on the NP surface, we believe that these NPs have greater potential to incorporate more avidin on its surface. One way to confirm this is to determine the level of avidin saturation for the NPs. After quantifying the amount of the avidin, we next calculated the number of biotin binding sites that may be available for ligand binding. Each avidin has four biotin binding sites; however, the binding sites are in close proximity to each other and the NP surface, which may lead to steric hindrance<sup>41</sup>. Hence, we assumed that only 2 biotin-binding sites per avidin molecule would be available for interaction with biotinylated-BAR.

To experimentally determine the ligand concentration required to saturate the available biotin binding sites, we reacted avidin-NPs and BAR-NPs with a 3-fold molar

excess of biotin-PEG-FITC (18.5 nmol/mg). Our results show that when biotin-PEG-FITC was reacted with avidin-NPs, biotin-PEG-FITC occupied only 65% (4.05 nmol/mg) of the available binding sites. This result suggests, that 18.5 nmol biotin-PEG-FITC per mg of avidin NP is not sufficient to saturate the available binding sites. When avidin-NPs were first reacted with 18.5 nmol/mg biotinylated-BAR and subsequently with biotin-PEG-FITC, only 2% of the biotin binding sites bound to biotin-PEG-FITC, suggesting that 98% of the available biotin binding sites were occupied by biotinylated BAR.

Since it was possible in the experiments above that 18.5 nmol biotin-PEG-FITC per mg avidin-NP was insufficient to saturate the biotin binding sites, a direct approach was used to quantify the amount of BAR bound to the NP surface using a fluorescein labeled peptide (BAR-Flc). For these experiments, BAR-Flc was reacted with avidin-NPs at a concentration range of 18.5, 37.1, 55.6 and 111.2 nmol/mg avidin-NPs (representing 3-, 6-, 9-, and 18-fold molar excess of BAR-Flc relative to the calculated biotin binding sites available) and NP bound fluorescence was determined. The results from this experiment were consistent with the indirect assay in that a 3-fold molar excess (18.5 nmol/mg) of BAR-Flc occupied approximately 62% of the available biotin sites. We previously assumed that each avidin molecule would only have 2 accessible biotin binding sites. From the microBCA, this assumption would indicate that 3.1 nmol/mg of avidin incorporated on the NP surface bind 6.2 nmol/mg of BAR. However, at an input concentration of 37.1 nmol/mg of BAR-Flc (6- fold molar excess), we discovered 7.4 nmol/mg of BAR-Flc was incorporated on the surface of avidin-NPs. This indicated that Avidin-NPs were saturated with BAR-Flc at an input concentration of 37.1 nmol/mg

avidin-NPs. Given this result, further conjugation reactions with BAR were carried out using 55.6 nmol of BAR-Flc per mg avidin-NPs and no significant additional BAR-Flc binding was observed. Together these results indicate that the assumption of two biotin binding sites was conservative and that few of the NPs had 3 available binding sites.

To assess the function of BAR-NPs, we compared the ability molar equivalent amounts of BAR peptide carried by BAR-NPs and soluble BAR to inhibit *P. gingivalis* adherence to *S. gordonii*. As shown in Figure 10, both soluble BAR and BAR-NPs inhibited *P. gingivalis* adherence in a dose dependent manner. However, BAR-NPs more potently inhibited *P. gingivalis* adherence relative to soluble BAR. The IC<sub>50</sub> of BAR-NPs was significantly lower (<0.3 μM) than soluble BAR (IC<sub>50</sub> 1.3 μM).

It is reported in many other studies that NPs that bind a large number of ligands show increased drug efficacy by promoting a multivalent binding interface<sup>41</sup>. In our experiments, we believe that BAR-NPs followed a similar mechanism of increased efficacy. In the future, we expect to develop mechanisms to identify the role that ligand number and ligand type plays in multivalent interaction between NP-ligands and a targeted receptor. Though the current approach does not provide comprehensive information about the binding kinetics of synthetic multivalent NPs, our analyses has an impact on the real-world biopharmaceutical development by providing a theoretical framework for designing future NPs that are better suited for targeting other microorganisms in oral biofilms. We also recognize that the etiology of periodontal disease is complex, and although recent evidence suggests that *P. gingivalis* may play an essential role in altering host-microbe homeostasis, other pathogens or pathogen interactions may have a significant impact on disease progression. Therefore, while these

delivery approaches will be initially applied to target BAR peptide to *P. gingivalis* niches, NPs might have broader applicability for targeting several other oral bacteria. This could be achieved for example, by co-modifying the surface of NPs with several other antimicrobial agents targeting other bacteria in the oral cavity. Furthermore, NPs could be co-modified with cell-surface adhesive proteins to increase retention times of these NPs in the oral cavity.

Our results suggest that BAR-NPs show a striking advantage at low concentrations and result in significantly higher inhibition of *P. gingivalis* adherence to *S. gordonii* than soluble BAR. We believe that the greater efficiency of BAR-NPs at lower concentrations can be helpful for the future development of therapeutic formulations such as a mouth rinse or chewing gum. In the oral cavity, the constant flow of saliva, the intake of food and water and other factors may reduce the levels of therapeutic NPs (i.e., wash out). Thus, the effectiveness of BAR may be reduced with time and approaches to increase the potency of the peptide. Due to the efficacy of BAR-NPs at both high and low concentrations, relative to soluble BAR, the beneficial activity of BAR may be well-suited to this open flow environment. Overall, our experiments show that we have a reliable and defined method of modifying NPs with inhibitory peptides. Our results suggest that nanotechnology can be efficiently used to combat oral pathogens and reduce oral diseases. It has been recently established that NPs are a proven platform for numerous infectious disease<sup>2</sup>. Hence the use of NP based drug delivery system to target specific organisms and niches in the oral microbiome represents a novel approach to combat periodontal disease.

Future studies will focus on developing alternative approaches of NP synthesis which incorporate more avidin per NP thereby further increasing the payload of BAR. Furthermore, assessing the efficacy of BAR-NPs by incorporating changes in the density of BAR surface modification. Furthermore, investigations will focus on the ability of BAR-NPs to reduce *P. gingivalis* virulence using the modified Baker mouse model of periodontitis. Together, the results from these experiments may provide proof-of-principle of the efficacy with which surface-modified targeted antimicrobial NPs can be utilized to control the complex biofilm associated with periodontal disease. Furthermore, additional studies will focus on synthesizing and characterizing targeted PLGA NPs that encapsulate BAR to provide an alternative platform that offers prolonged-release of the peptide. Following this, experiments will be done to examine the toxicity of modified and sustained release NPs against human oral gingival and innate immune cells, and methods to formulate NP preparations. The long-term goal is to develop a formulation that can be tested for efficacy in clinical trials.

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## PRESENTATIONS

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Nov 2015, Sep 2014

Poster Presentation: Synthesis and Functional Evaluation of Peptide-Modified Poly(Lactic-co-Glycolic Acid) Nanoparticles to Inhibit *Porphyromonas gingivalis* Biofilm Formation

23<sup>rd</sup> Indiana University Research Day, Indianapolis, IN

April 2015

Poster presentation: Synthesis and Functional Evaluation of Peptide-Modified Poly(Lactic-co-Glycolic Acid) Nanoparticles to Inhibit *Porphyromonas gingivalis* Biofilm Formation

IADR/AADR/CADR General session and exhibition, Boston, MA

March 2015

Poster presentation: Synthesis and Functional Evaluation of Peptide-Modified Poly(Lactic-co-Glycolic Acid) Nanoparticles to Inhibit *Porphyromonas gingivalis* Biofilm Formation

20<sup>th</sup> Hinman Student Research Symposium, Memphis, TN

Oct 31<sup>st</sup> - Nov 2<sup>nd</sup> 2014

Poster Presentation: Synthesis and Functional Evaluation of Peptide-Modified Poly(Lactic-co-Glycolic Acid) Nanoparticles to Inhibit *Porphyromonas gingivalis* Biofilm Formation

Gyandeeep Interstate Dental Convention, Vadodara, Gujarat, India

March 2012

Paper Presentation: Nano Medicine: Developing Smarter Periodontal Therapeutics

4<sup>th</sup> Indo-Australian Conference on Biomaterials and Drug Delivery System, Anand, Gujarat, India

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Poster Presentation: Novel Biomaterials in Periodontal Regeneration